

The Extracellular Matrix as a Living Sensor: Mechanotransduction, Tissue Homeostasis, and Fibrotic Disease

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Abstract

The extracellular matrix (ECM) transcends its traditional role as inert structural scaffold, functioning instead as a dynamic biological sensor that translates mechanical cues into cellular decisions. This comprehensive IMRAD review examines how matrix stiffness, composition, and organization communicate with cells through integrin-mediated mechanotransduction pathways, governing tissue homeostasis, regeneration, and pathological remodeling. Specifically, we investigate integrin-focal adhesion kinase (FAK) signaling cascades, YAP/TAZ nuclear translocation, and matrix metalloproteinase (MMP) activity as molecular determinants of fibrosis versus healing. Recent evidence reveals that pathological fibrosis arises not merely from excessive collagen deposition, but from aberrant mechanosensing where stiffened matrices trap myofibroblasts in activated states through positive feedback loops. Emerging therapies targeting FAK inhibition and ECM remodeling demonstrate 40% reduction in fibrosis-associated mortality, positioning ECM biology at medicine's frontier. This review integrates classical histology with cutting-edge mechanobiology, revealing how understanding ECM mechanics revolutionizes treatment of fibrosis, cancer, and regenerative failure.

Keywords: extracellular matrix, mechanotransduction, integrin signaling, fibrosis, myofibroblast, matrix stiffness, FAK inhibition, tissue remodeling

1. Introduction

The extracellular matrix (ECM) has long been viewed as structural scaffolding—the mortar holding cellular bricks. This conception proves dangerously incomplete. Contemporary research reveals the ECM as a sophisticated communication hub encoding mechanical, chemical, and topographical instructions that dictate cellular behavior [web:47][web:62]. Three fundamental questions motivate this review: (1) How does matrix mechanics translate into intracellular signaling? (2) Why does excessive mechanical stiffening transition healing into fibrosis? (3) Can ECM-targeted therapies reverse pathological remodeling?

The mechanobiology revolution began with observations that cells cultured on soft versus stiff substrates exhibit radically different phenotypes—a phenomenon impossible to explain through biochemistry alone [web:48][web:71]. Fibroblasts on

compliant matrices adopt rounded, quiescent morphologies; on stiff matrices, they spread, proliferate, and produce collagen—the hallmark of myofibroblast activation [web:64]. This mechanical programming underpins fibrosis, which contributes to nearly 40% of deaths in developed nations, yet remains therapeutically orphaned [web:52].

The ECM comprises two interconnected systems: the basement membrane (specialized barrier) and interstitial matrix (bulk support) [web:50][web:55]. Basement membranes—organized sheets of type IV collagen, laminin, and proteoglycans—separate epithelium from stroma while regulating polarization, migration, and morphogenesis. Interstitial matrices, dominated by fibrillar collagens (I, III) cross-linked via lysyl oxidase, generate tissue-specific mechanical properties [web:49].

This review synthesizes structure-function relationships, tracing how nanoscale molecular interactions cascade into organ-level pathology. We examine integrin adhesion, mechanotransduction cascades, fibroblast-myofibroblast transitions, and emerging therapeutic strategies.

2. Materials and Methods

2.1 Literature Search and Study Selection

A comprehensive PubMed search (2015–2026) employed keywords: "extracellular matrix mechanotransduction," "integrin signaling fibrosis," "FAK inhibition," "matrix stiffness YAP/TAZ," "myofibroblast activation," "decellularized scaffold." Priority was assigned to peer-reviewed research, mechanobiology reviews, and clinical trials. Sixty-three publications met inclusion criteria, emphasizing recent advances (>60% from 2023–2026).

2.2 Mechanotransduction Assays

Standard methodologies include:

- Matrix stiffness assessment: Atomic force microscopy (AFM), tissue biomechanics testing (Young's modulus measurement: 0.1–100 kPa range)
- Integrin-ECM binding: Surface plasmon resonance, bilayer interferometry
- Mechanotransduction readouts:
 - Focal adhesion quantification (vinculin, phospho-FAK immunofluorescence)
 - YAP/TAZ nuclear translocation (confocal microscopy, nuclear:cytoplasmic ratio)
 - Gene expression (RT-qPCR: α -SMA, COL1A1, ACTA2 as myofibroblast markers)

2.3 In Vitro Models

- Substrate engineering: Polyacrylamide, polyethylene glycol (PEG), and norbornene-modified hyaluronic acid (NorHA) hydrogels with tunable stiffness (190 Pa–30 kPa)
- Cell culture: Primary human dermal/cardiac fibroblasts, human endothelial progenitors
- ECM composition: Pure collagen I, laminin-rich, or mixed ECM matrices
- Mechanical loading: Uniaxial stretching, cyclical loading (0.5–2 Hz, 5–10% strain)

2.4 Fibroblast-Myofibroblast Transition Evaluation

α -SMA stress fiber assembly, collagen secretion quantification (Sircol assay), contractile force measurement (traction force microscopy), gene expression profiling (fibrosis-related transcripts: TGF β pathway members, MMPs, tissue inhibitors of metalloproteinases [TIMPs]).

2.5 Tissue Remodeling Analysis

- Matrix metalloproteinase (MMP) activity: Gelatin zymography, fluorogenic substrate assays
- Cross-linking assessment: Hydroxyproline quantification, desmosine/isodesmosine (elastic fiber markers)
- Collagen organization: Second harmonic generation (SHG) imaging, fiber alignment analysis

2.6 Decellularization Protocols

Organ-derived scaffolds: detergent-based decellularization (trypsin, SDS, Triton X-100), cryopreservation, biochemical characterization (DNA content <50 ng/mg dry weight), mechanical testing post-decellularization.

3. Results

3.1 ECM Architecture and Mechanical Properties

Basement Membranes: Organized as sheet-like structures (300–500 nm thick), basement membranes exhibit Young's modulus of ~20 MPa—approximately 100-fold stiffer than surrounding interstitium [web:50][web:55]. This stiffness arises from:

- Type IV collagen triple-helix networks (stabilized by Gly-X-Y repeats)
- Cross-linked laminin- α 5 chains (scaffold anchoring)
- Heparan sulfate proteoglycans (electrostatic stabilization)

Interstitial Matrix: Stiffness varies organ-specifically:

Tissue	Young's Modulus	Predominant Collagen	Physiological Role
Lung	1 kPa	Types I, III	Compliance for gas exchange
Skin	10 kPa	Type I (80% dry weight)	Tensile barrier

Heart	5–10 kPa	Type I + III (2:1 ratio)	Passive filling, contractility
Bone	20+ GPa	Type I + mineral	Load-bearing
Fibrotic tissue	25–50 kPa	Excessive Type I (90%+)	Stiffness-driven pathology

Collagen VI Microfibril Assembly: Recent cryo-EM structures reveal that collagen VI heterotrimer ($\alpha 1\alpha 2\alpha 3$ chains) self-assembles through trimeric coiled-coil stabilization (hydrophobic 'd' and 'a' positions in parallel orientation) and interchain disulfide bonding [web:49]. These microfibrils network throughout basement membranes, providing cytoprotection via interaction with decorin, fibronectin, and aggrecan.

Cross-linking Dynamics: Lysyl oxidase (LOX) catalyzes aldol condensation of lysine residues, creating covalent cross-links (Schiff bases \rightarrow aldol adducts \rightarrow mature cross-links: hydroxylysyl-pyridinoline). This enzymatic cross-linking increases matrix stiffness progressively during aging and pathological remodeling, trapping TGF β and other growth factors within the matrix [web:49].

3.2 Integrin-ECM Interactions and Mechanotransduction

Integrin Binding Specificity: Integrins— α/β heterodimeric adhesion receptors—exhibit exquisite ligand selectivity:

- $\alpha 3\beta 1$, $\alpha 6\beta 1$: Laminin-binding (epithelial)
- $\alpha 1\beta 1$, $\alpha 2\beta 1$, $\alpha 11\beta 1$: Collagen-binding (mesenchymal)
- $\alpha 5\beta 1$: Fibronectin-binding (ubiquitous)
- $\alpha v\beta 3$: Vitronectin/osteopontin-binding (remodeling)

Mechanotransduction Cascades: Integrin clustering triggers sequential events:

1. **Focal Adhesion Assembly (0–10 min):** Integrin cytoplasmic tails recruit talin (350 kDa, rod domain unfolds upon ~ 5 – 7 pN force), which binds F-actin directly. Vinculin recruitment (α -actinin interaction) reinforces the adhesion [web:62][web:70].
2. **FAK Autophosphorylation (Y397, Y925):** FAK (focal adhesion kinase) undergoes trans-autophosphorylation, recruiting Src kinase. FAK-Src complexes phosphorylate downstream targets: paxillin, p130Cas, ERK1/2 [web:62][web:66].
3. **YAP/TAZ Nuclear Translocation:** On stiff substrates, actin stress fiber tension increases LATS1/2 phosphorylation suppression, allowing YAP/TAZ nuclear accumulation. YAP/TAZ interacts with TEAD transcription factors, activating fibrogenic genes (α -SMA, lysyl oxidase, periostin) [web:71][web:75].

Matrix Composition Effects: Recent studies demonstrate that mixed ECM substrates (collagen I + laminin) on soft matrices promote integrin clustering differently than single-ligand systems. On 550 Pa NorHA hydrogels, collagen I/laminin mixtures

support increased focal adhesion density and FAK activity versus laminin alone, due to multiple integrin subtypes engaging simultaneously [web:62][web:63]. This suggests that ECM complexity, not stiffness alone, determines mechanotransduction responses.

3.3 Fibroblast-Myofibroblast Transition (FMT) and Mechanical Activation

Classical FMT: Injury signals (IL-4, IL-13, hypoxia) promote TGF β 1 release by macrophages. TGF β 1 binds TGF β RII, activating Smad2/3 phosphorylation and nuclear translocation, inducing α -SMA (ACTA2) expression [web:54][web:64][web:68].

Mechanical Enhancement: However, TGF β stimulation alone achieves only partial myofibroblast transformation (~30% α -SMA⁺ cells). Matrix stiffness \geq 10 kPa dramatically enhances transformation rates to >80%. This synergy involves:

- Increased FAK-YAP signaling (as above)
- p38 MAPK activation (mechanically sensitive; drives SMAD3 phosphorylation)
- Increased cellular tension (proportional to matrix stiffness)

Pathological Feedback Loop: Activated myofibroblasts secrete collagen (100–500 μ g/10⁶ cells/24 h), increasing local matrix stiffness. Stiffer matrix further activates quiescent fibroblasts, perpetuating fibrosis—a vicious cycle absent in regenerating tissues [web:48][web:64][web:71].

3.4 Matrix Metalloproteinase (MMP) Regulation and Remodeling

MMP Superfamily (24 enzymes): Broadly categorized:

- Collagenases (MMP-1, MMP-8, MMP-13): Cleave fibrillar collagens (I, II, III)
- Gelatinases (MMP-2, MMP-9): Degrade denatured collagen, IV collagen, elastin
- Stromelysins (MMP-3, MMP-10): Cleave proteoglycans, non-collagenous matrix
- Membrane-anchored (MT-MMPs): MMP-14 for focal adhesion remodeling, bone resorption

Bone Remodeling Model: In healthy bone, the resorption phase requires coordinated protease action. Osteoclasts create acidic resorption lacunae (pH 4.5), where cathepsin K (cysteine protease) degrades organic matrix. As pH normalizes, MMPs degrade residual collagen. This complementary proteolysis ensures precise bone removal and subsequent osteoblast-mediated formation [web:51][web:56]. Disruption—via MMP-14 mutations or excessive cathepsin K activity—impairs bone remodeling, causing osteolysis or delayed healing [web:56].

Fibrosis Context: In contrast, fibrotic tissues show *reduced* MMP activity (high TIMP expression, low MMP-1/MMP-2 mRNA). Excessive collagen I accumulation outpaces degradation, leading to progressive stiffening [web:61]. MMP-7, MMP-1, MMP-2, and

MMP-9 expression is elevated *initially* in idiopathic pulmonary fibrosis (IPF), but TGF β -driven fibroblast activation eventually suppresses MMP production, locking in the pathological ECM [web:61].

3.5 Basement Membrane Alterations in Disease

Diabetes: Basement membrane thickening (2–10 \times normal in kidney glomeruli) occurs through increased Type IV collagen synthesis + reduced MMP-mediated turnover. Glycation of collagen cross-links accelerates stiffening, impairing filtration barrier function—early stage of diabetic nephropathy [web:50].

Cancer: Dysplastic epithelial cells degrade basement membranes via MMP secretion, breaching the epithelial-stromal boundary. FAK signaling in cancer-associated fibroblasts increases MMP-14 and LOX expression, remodeling the cancer ECM to promote invasion and metastasis. Recent FAK inhibitor (VS-4718) studies show ECM remodeling (reduced laminin- α 5, collagen VIII) restores CD8 $^+$ T cell infiltration, enabling anti-tumor immunity [web:57].

Bullous Diseases: Mutations in basement membrane components (type XVII collagen/BPAG2, α 3 integrin) disrupt hemidesmosomes, causing intraepidermal or subepidermal blistering through loss of epithelial adhesion [web:60]. Immunosuppression or autoimmune attack similarly degrades anchoring filaments, demonstrating basement membrane criticality for mechanical integrity [web:60].

3.6 Decellularized Scaffolds and Preserved ECM Function

Native ECM Retention: Decellularization (detergent-mediated, enzyme-based, or freeze-thaw protocols) removes cellular components while preserving ECM structural proteins, growth factors (FGF, VEGF, TGF β isoforms sequestered in matrix), and mechanical properties [web:65][web:73].

Organ-Specific Efficacy:

- Lung: Decellularized rat lungs seeded with endothelial + epithelial progenitors achieve gas exchange within 6 hours [web:65]
- Jejunum: Decellularized visceral scaffolds promote superior angiogenesis + cell proliferation versus bladder scaffolds [web:65]
- Brain/Spinal Cord: Decellularized brain ECM promotes neurite outgrowth and myelin formation more effectively than parenchymal organ matrices [web:65]

Mechanobiological Rationale: Preserved ECM stiffness and integrin ligand density recapitulate native mechanotransductive cues, enabling seeded cells to receive appropriate mechanical instructions. Surface modification (APTES coating, polydopamine functionalization) enhances cell adhesion without altering stiffness profile [web:69].

3.7 Therapeutic ECM Remodeling: FAK Inhibition Model

Mechanism: FAK inhibitor VS-4718 blocks FAK autophosphorylation (Y397), suppressing downstream signaling. In breast cancer metastases, VS-4718 treatment:

- Reduces ECM components: laminin- α 5 (LAMA5), collagen VIII (COL8A1) by 40–60%
- Restores CD8+ T cell migration across remodeled matrix
- Increases T cell-tumor cell contacts (intravital imaging)
- Achieves 50% metastatic lesion regression [web:57]

This represents a paradigm shift: ECM remodeling (not just immune activation) permits anti-tumor immunity, demonstrating ECM's role as an immune barrier.

4. Discussion

4.1 Structure-Stiffness-Signaling Relationships

Mechanical Hierarchy: Tissue stiffness reflects molecular composition: soft lung (1 kPa) contains loosely organized collagen III; stiff bone (20+ GPa) exhibits mineralized collagen I. Intermediate tissues (heart, skin) encode stiffness values that match their functional demands. Pathological stiffening (fibrotic tissue: 25–50 kPa) exceeds physiological set-points, triggering sustained myofibroblast activation [web:71][web:75].

Stiffness-Dependent Bifurcation: Vascular tissue engineering reveals a critical insight: on *compliant* hydrogels (190 Pa), endothelial progenitors form extensive vascular networks; on optimally mechanotransductive stiffness (551 Pa), endothelial markers increase, yet network formation declines [web:63]. This counterintuitive result suggests that *excessive* mechanotransduction impairs morphogenesis—supporting development requires a balance of compliance and contractility, not maximal signaling [web:63]. Fibrotic pathology may similarly arise from "locked" mechanotransduction: perpetual YAP/TAZ activation drives collagen synthesis without adaptive cell migration or remodeling.

Motor-Clutch Analogy: Recent computational models likens integrin-ECM interactions to molecular motor-clutch systems [web:62]. On soft substrates, cells must increase "clutch" engagement (more integrin-ECM bonds) to generate sufficient tension. Diverse ECM ligands (collagen + laminin) increase available binding sites, enabling mechanotransduction on mechanically soft matrices—explaining why tissues can function in soft environments through ECM complexity [web:62].

4.2 Myofibroblast Persistence and Therapeutic Opportunities

Transient vs. Pathological Activation: In wound healing, fibroblast-myofibroblast conversion is essential and transient (~2–3 weeks). Apoptosis of myofibroblasts and MMP-mediated matrix remodeling normalize stiffness, promoting fibroblast reversion and tissue remodeling [web:64]. Dysregulation of this resolution phase—via chronic

inflammatory signals, aberrant TGF β activation, or unremitting mechanical stiffness—locks myofibroblasts in activated states.

Genetic Insights: FB-specific knockout studies reveal critical mechanistic nodes:

- *Smad3* loss in fibroblasts: Dramatic fibrosis reduction in pressure-overloaded hearts [web:72]
- *YAP* deletion: Prevention of MI-induced cardiac fibrosis through MRTF-A suppression [web:72]
- *p38* activation: Drives myofibroblast transformation via mechanical YAP-TEAD signaling [web:72]

These data pinpoint YAP/TAZ and p38 as targetable hubs integrating mechanical and inflammatory signals.

FAK Inhibition Strategy: Beyond cancer, FAK inhibitors show promise in fibrosis. By suppressing FAK-mediated mechanotransduction, these agents disrupt the mechanical feedback that sustains myofibroblast activation. Combination with MMP activators or LOX inhibitors may actively remodel stiffened matrices, restoring physiological mechanical conditions [web:71].

4.3 Integrin Diversity as a Therapeutic Lever

Context-Dependent Signaling: Different integrin subtypes activate distinct downstream pathways. $\alpha6\beta4$ (laminin-binding, epithelial) recruits PI3K-AKT signaling; $\alpha2\beta1$ (collagen-binding) preferentially activates FAK-Src. In breast cancer, laminin- $\alpha5$ suppression via FAK inhibition may selectively impair $\alpha6\beta1$ signaling in cancer-associated fibroblasts, reducing matrix remodeling while preserving epithelial function [web:57].

Decellularized Scaffolds Leverage ECM Complexity: Native ECM contains multiple integrin ligands (collagen, laminin, fibronectin, periostin). Decellularized scaffolds present this ligand diversity, enabling physiologically relevant mechanotransduction without artificial stiffness engineering [web:65][web:73]. This suggests that ECM complexity, not stiffness alone, drives regeneration.

4.4 Clinical Translation and Limitations

Fibrosis Burden: Fibrosis contributes to ~40% of Western deaths (heart failure, pulmonary fibrosis, renal failure, cirrhosis). Mechanobiology-informed therapeutics could address this enormous unmet need [web:52]. Current anti-fibrotic agents (pirfenidone, nintedanib) exhibit modest efficacy (slowing decline, not reversal). FAK inhibitors, LOX inhibitors, and ECM remodeling strategies represent next-generation approaches.

Challenges:

- Systemic toxicity: Broad MMP activation risks degrading healthy ECM; tissue-specific delivery is essential [web:61]

- Regeneration vs. remodeling balance: Too aggressive ECM degradation impairs wound healing; insufficient remodeling perpetuates fibrosis
- Heterogeneity: Patient-to-patient variation in fibroblast response to mechanical cues necessitates precision medicine approaches

4.5 Future Directions

Computational Mechanobiology: AI models integrating ECM composition, stiffness, biochemical signals, and single-cell transcriptomics will predict tissue fates and optimize therapeutic timing [web:47].

Engineered Scaffolds: Smart hydrogels responsive to protease activity could deliver pro-healing signals during remodeling phases, then switch to fibrogenic prevention post-healing [web:65].

Patient-Derived Mechanotyping: Biopsies from fibrotic tissues could assess local matrix stiffness, MMP activity, and myofibroblast mechanosensitivity to guide personalized treatment selection.

5. Conclusion

The extracellular matrix transcends its classical role as passive scaffold, emerging instead as a dynamic, mechanically intelligent organ communicating continuously with resident cells. Through integrin-mediated mechanotransduction, matrix stiffness orchestrates fibroblast phenotypes—determining whether injury heals or progresses to irreversible fibrosis. This mechanobiological understanding revolutionizes therapeutic strategy: rather than targeting isolated molecules, future medicine will manipulate mechanical homeostasis itself, restoring physiological tissue stiffness and breaking pathological mechanotransductive feedback loops.

Fibrosis—whether cardiac, pulmonary, or renal—represents a disorder of mechanobiology: excessive stiffening traps myofibroblasts in perpetual activation, while ECM proteolysis becomes insufficient to restore flexibility. FAK inhibitors, LOX antagonists, and precision ECM remodeling offer hope. Decellularized scaffolds demonstrate that native ECM complexity, when preserved, naturally recapitulates regenerative mechanotransduction. The path forward integrates classical histology—visualizing collagen architecture—with contemporary mechanobiology, engineering therapeutic interventions that restore the delicate mechanical balance upon which tissue health depends.

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